

# Bioresorbable stents: The future of interventional cardiology?

## ■ ABSTRACT

The introduction of stents has drastically reduced target-lesion restenosis rates associated with percutaneous coronary angioplasty. Bare-metal stents were the first introduced, followed by drug-eluting stents, both of which had significant impacts on the complication rates. Stents, however, have resulted in the emergence of stent thrombosis and stent restenosis, which can cause life-threatening cardiac complications. Three new technological approaches are being investigated to overcome these complications: stents coated with bioresorbable polymers, stents without polymers, and completely bioresorbable stents. Initial results are encouraging, but more data are needed to ascertain their implications for clinical practice.

## ■ KEY POINTS

Stents have dramatically improved outcomes associated with percutaneous coronary angioplasty.

Bare-metal stents were the first stents developed, followed by first- and second-generation drug-eluting stents, which have progressively reduced complication rates.

Despite the improvements with conventional stents, persistent rates of restenosis and stent thrombosis remain, which can lead to increased coronary morbidity and mortality.

New stent technologies include stents coated with bioresorbable polymers, stents without polymers, and completely bioresorbable stents.

Interventional cardiology has made great strides in the last few decades. Percutaneous coronary intervention (PCI) is among the most commonly performed medical procedures globally.<sup>1</sup> At the time of inception, PCI was plagued by high complication rates—balloon catheters had a 50% target-lesion restenosis rate at 6 months and required emergency bypass surgery in up to 6% patients.<sup>2</sup> With passage of time, the complication rate of PCI has markedly decreased.

The introduction of stents had a dramatic impact on lowering the complication rates. Initially, the bare-metal stents (BMS) reduced the stent restenosis rate to 10% to 15%. Drug-eluting stents (DES) have further revolutionized the field (**Figure 1**), significantly lowering rates of stent thrombosis (less than 0.5% in 1 year) and risk of restenosis (less than 5% in 1 year).<sup>3–6</sup> The second-generation DES widely used in contemporary practice have made even more reductions owing to their improved designs and metallic and polymer composition; and concurrent advancements in the medical management, including use of antithrombotic and antiproliferative drugs, have further contributed to improved rates.

What, then, is to be hoped for? Unfortunately, with the advent of stents, complications such as stent thrombosis and stent restenosis also emerged. These complications can be life-threatening in the form of post-procedural or late myocardial infarction and cardiac death. Thus, although the US Food and Drug Administration (FDA) assesses target-lesion failure (defined as a composite of cardiac death, target vessel myocardial infarction, or ischemia-driven target vessel revascularization) at 1 year, patients can have complications for the remainder of their lives. Despite the advancements attained by the second-generation DES over their predecessors, the issue of stent thrombosis and restenosis continues to plague second-generation DES with a 2% to 2.5% increased rate of target-lesion failure each year, seemingly forever (**Figure 2**).<sup>7,8</sup>

This article will briefly discuss the stent design and pathophysiology driving stent thrombosis and restenosis along with potential strategies to mitigate

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the problem. It pays special emphasis to bioresorbable stents, given their increasing interest among interventional cardiologists and patients, and given their potential to transform the practice of PCI.

### STENT DESIGN

Contemporary DES essentially consist of three components:

- A metallic alloy with a mesh-like design serves as the platform for the stent.
- This framework is coated with a multi-layered polymer that holds and releases the active drug in a controlled manner so that its effects can be extended.
- An antiproliferative drug (absent in the bioresorbable stents) that inhibits the smooth muscle proliferation and neointimal hyperplastic response: sirolimus or paclitaxel in first-generation DES; everolimus or zotarolimus in second-generation DES (Figure 3).

### WHAT CAUSES STENT THROMBOSIS AND RESTENOSIS?

Several theories and pathophysiological mechanisms have been proposed to explain these late adverse events (Table 1). However, our overall understanding of the cause remains modest at best. The major factor seems to be persistent presence of polymer on the stent and the ensuing inflammation. The second issue appears to be related to neoatherosclerosis that is generally defined as lipid or calcified neointima. Neoatherosclerosis is especially problematic for the second-generation DES. Neoatherosclerosis eventually predisposes to the development of thin cap fibroadenoma, and the rupture of thin cap leads to stent thrombosis and restenosis.

Autopsy studies suggest that approximately 50% of first- and second-generation DES start developing neoatherosclerosis within 1 to 3 years of implantation.<sup>9</sup> Turbulence created by thick strutted stents or incomplete impaction of stents to the vessel

wall predisposes the stents to platelet aggregation and fibrinogen deposition, thereby increasing the risk of neoatherosclerosis. Despite these pathologic insights, no treatment strategy has been shown to attenuate the problem, with the exception of high-dose statins.

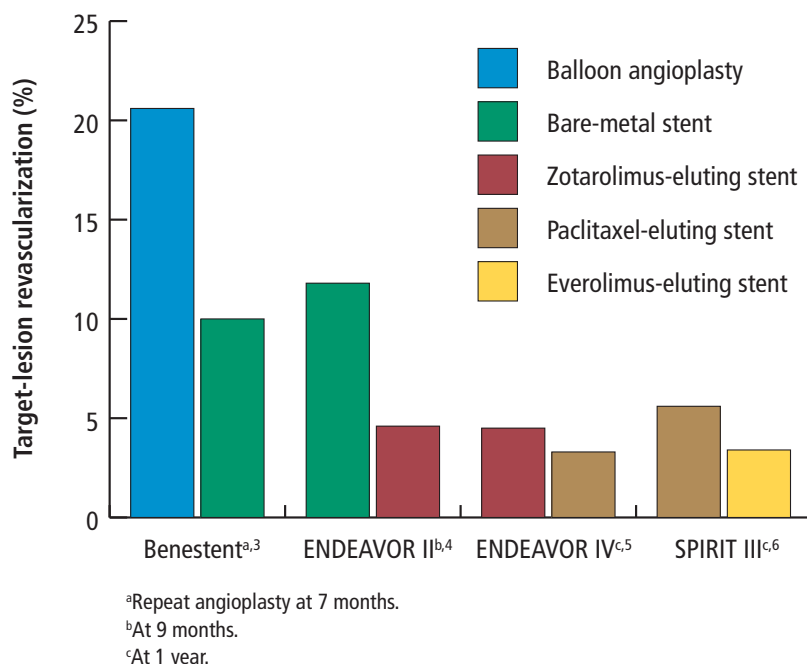


FIGURE 1. Reduction of restenosis rates by stent type.

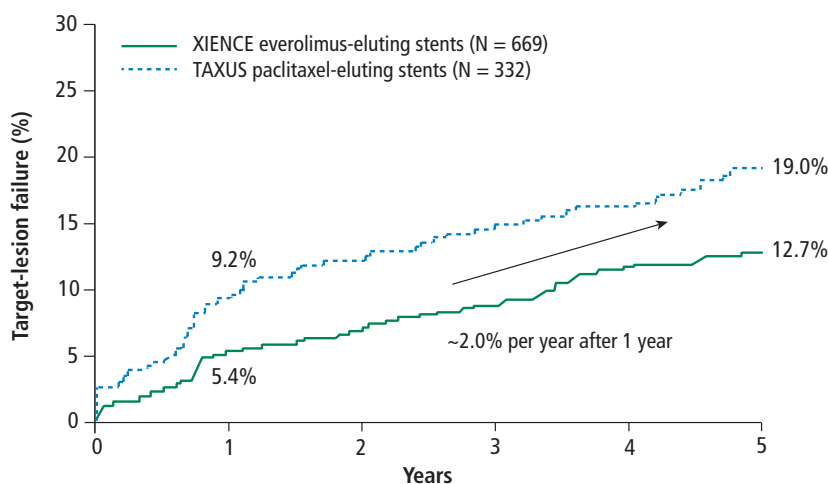
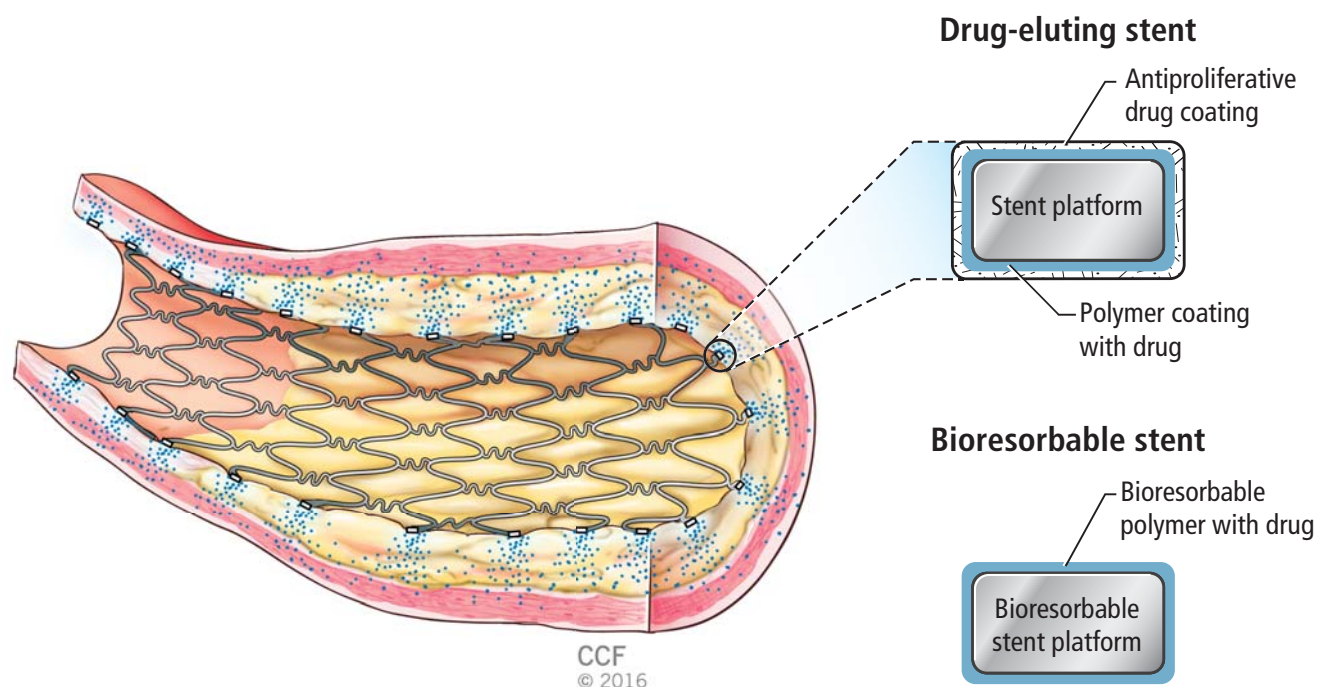


FIGURE 2. Second- vs first-generation drug-eluting stents.

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**FIGURE 3.** Components of drug-eluting and bioresorbable stents.

## ■ CAN WE SOLVE THE PROBLEM?

Three technological approaches have been proposed to overcome stent thrombosis and restenosis:

- Stents coated with bioresorbable polymers that quickly degrade
- Stents without polymers
- Stents that are completely resorbed.

## ■ STENTS WITH BIORESORBABLE POLYMERS

As described above, the presence of a polymer on the stent predisposes it to inflammation. Therefore, it would be logical to hypothesize that a bioresorbable polymer would reduce the inflammation. This approach is typified by the second-generation paclitaxel-eluting stent (Synergy, Boston Scientific). It has a biodegradable coating that resorbs within 4 months and releases everolimus in a dose intensity similar to that seen with the contemporary second-generation DES.

The largest trial of this device to date, the Evolve II study, randomly assigned 1,684 patients to the bio-stable-polymer, everolimus-eluting chromium stent (Promus, Boston Scientific) or the paclitaxel-eluting stent (Synergy, Boston Scientific).<sup>10</sup> Two-year follow-up data suggest that the rate of target-lesion failure was 9.4% in the paclitaxel-eluting stent patients vs 8.5% in the everolimus-eluting stent patients.

Notably, no definite stent thrombosis was seen in the Synergy-treated patients 24 hours after the initial device implantation.

## ■ STENTS WITHOUT POLYMERS

If polymers predispose to inflammation, stents without polymers should mitigate the risk. Such stent types are exemplified by the BioFreedom (Biosensors International) stainless steel stent, a polymer-free urokinase (also known as biolimus A9)-eluting stent. These stents have a microstructured surface that holds the drug without a polymer and releases the active drug over a few months.

The LEADERS FREE clinical trial studied this stent in 2,466 patients at high risk of bleeding.<sup>11</sup> The patients were randomized to receive either a BMS or the polymer-free stent. All patients were required to receive dual antiplatelet therapy for only 1 month. At 1 year, the composite risk of cardiac death, myocardial infarction, and stent thrombosis was 9.4% in patients with BioFreedom stents vs 12.9% in BMS patients. Of note, the primary end point did not include stent restenosis, thereby not disadvantaging the BMS.

Medtronic's polymer-free, sirolimus-eluting stent is currently under investigation in the RevElution clinical trial.<sup>12</sup> It has a cylindrical structure with the

core replaced by the active drug sirolimus. Abluminal holes in the stent allow controlled release of the drug. A pharmacokinetic analysis shows that 90% of the medication is released within the first 90 days and that tissue concentrations are maintained in the therapeutic range until at least that time.<sup>13</sup> This actually exceeds that of the second-generation everolimus-eluting DES.

## ■ BIORESORBABLE STENTS

Bioresorbable scaffolds or stents disappear entirely over time and have drawn considerable attention in the interventional cardiology community. The FDA recently approved Abbott's Poly-L-Lactic Acid (PLLA) everolimus-eluting stent (Absorb). The rate of bioresorption of this device can be controlled by modulating the respective contribution of amorphous and crystalline PLLA backbone. The advantage of bioresorbable stents appears to stem from the fact that with bioresorbable devices, the vessel may actually expand and the purported nidus for inflammation goes away. This has been demonstrated by serial intravascular ultrasound-based studies.<sup>14</sup>

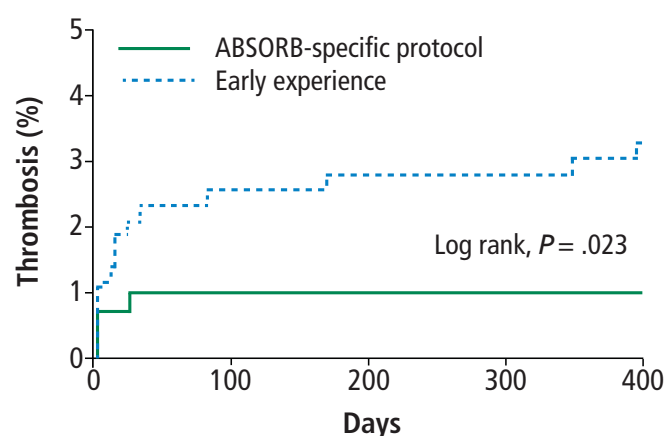
The return of pulsatility also appears to modulate the transition of smooth muscles from proliferative back to their contractile phenotype. This has been hypothesized to reduce the risk of neoatherosclerosis and, consequently, stent restenosis. The limitation of this device is the large strut size (157 micron for Absorb vs 81 microns for Xience). Dissolving metallic scaffolds also tend to have thicker struts than the current DES (120 vs approximately 80 microns).

The Absorb III trial was a pivotal noninferiority US trial that led to the device approval.<sup>15</sup> In this trial, 2,008 patients were randomized to receive the Absorb bioresorbable, everolimus-eluting stent or the DES Xience. The primary study end point was target-lesion failure at 1 year. As is often the case with US landmark studies, patient and lesion complexities were limited. Patients with acute

**TABLE 1**

**Construction of first- and second-generation drug-eluting stents (DES) and proposed pathophysiological mechanism of late adverse events**

	Construction	Mechanism
First-generation DES	Thick struts Uneven polymer distribution with poor integrity and thick coating of durable polymers High drug dose	Uncovered struts Hypersensitivity Malapposition from fibrin deposition Stent fracture Neoatherosclerosis (especially for second-generation DES)
Second-generation DES	Thinner struts More biocompatible polymer (durable) Reduced drug dose	



Patients (N)					
Early experience	369	369	369	369	369
ABSORB-specific	292	292	281	217	155

**FIGURE 4.** ABSORB learnings: MICAT. Pre-dilation with noncompliant balloon sized 1:1 to normal vessel with complete balloon expansion; post-dilation at 14–16 atmospheres.

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coronary syndrome, elevated cardiac enzymes, high-risk anatomic lesions such as bifurcation lesions, and chronic total occlusion were excluded. Patients with diabetes comprised less than one-third of the patients, and lesions were relatively short at  $13 \pm 6$  mm.

Device success per lesion was lower with Absorb than with Xience (94.3% vs 99.3%;  $P < .0001$ ). This



**TABLE 2**

**Key elements of technique with the Absorb scaffold**

Properly choose the lesion
<ul style="list-style-type: none"> <li>Definitely <math>\geq 2.5</math>–<math>3.75</math> mm in diameter (if in doubt, check intravascular ultrasound or optical coherence tomography)</li> <li>No excessive tortuosity or calcium proximal</li> </ul>
Prepare the lesion by 1:1 predilation and confirm $< 40\%$ diameter residual stenosis
Post-dilate with 1:1 noncompliant balloon at $\geq 14$ atmospheres
Pay attention to expansion limits
<ul style="list-style-type: none"> <li>Oversizing the scaffold by a balloon <math>&gt; 0.5</math> mm the scaffold diameter risks strut fracture</li> </ul>
Prescribe dual antiplatelet therapy

is likely due to the larger strut size. Absorb III did meet the prespecified primary end point for noninferiority ( $P = .007$ ), although the rate of adverse events was somewhat higher (7.8% vs 6.1%). A subgroup analysis reveals that 19% of all lesions were smaller than what was originally intended, and in these patients, the Absorb device performed poorly with a 4.6% risk of device thrombosis. When limited to patients with the intended reference vessel sizes, the results of target-lesion failure and stent thrombosis were similar (6.6% vs 5.5% and 0.8% vs 0.5%, respectively).<sup>15</sup>

The implantation technique also seems to have influenced the results, with increased use of post-dilation as the study evolved. Recent observations from the MICAT group have shown that the use of high pressure post-dilation and other procedural advancements may considerably reduce adverse outcomes associated with Absorb (Figure 4).<sup>16</sup> Thus, while the pooled analysis in the form of a meta-analysis has suggested an increased risk of device thrombosis,<sup>17</sup> the difference is attenuated by selecting lesions of appropriate size, high-pressure post-dilation, and procedural advancements (Table 2).

## CONCLUSION AND THE WAY FORWARD

Current first-generation bioresorbable stents can achieve results similar to those of second-generation DES, provided that they are used in patients with noncomplicated coronary lesions and the implant techniques are optimized. We do not know the outcomes of bioresorbable stents in patients with complex lesions. Current experience suggests that other changes in technique would be needed. For example,

minimizing scaffold overlap in long and bifurcating lesions. Whether that would translate into diminishing the rate of late adverse events remains to be determined. As of now, we only have data on approximately 100 highly selected patients beyond 3 years (no adverse events 2.5 to 5 years after implantation).

Several investigational second-generation bioresorbable stents, including Elixir's Dissolve PLLA, Boston Scientific's FAST, and a newer version of Absorb, are in early clinical trials. Smaller strut thickness holds the promise of attenuating the risk of stent thrombosis. Since the polymer persists, no reduction in dual antiplatelet therapy duration is likely to be achieved.

Results from long-term follow-up of Absorb III and on-going trials are eagerly awaited to ascertain whether the rate of late complications of DES can be mitigated. It would not be surprising if the second-generation bioresorbable stents make DES a thing of the past within the next decade.

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